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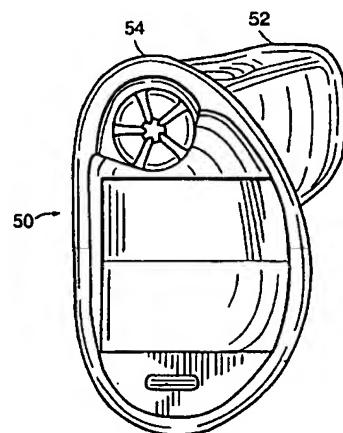
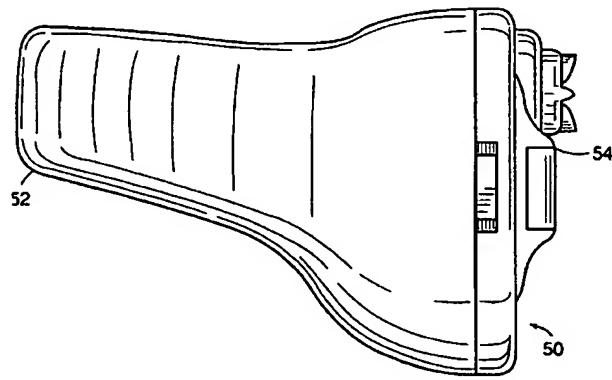
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[Continued on next page]

(54) Title: COCHLEAR IMPLANT SYSTEM PARTIALLY INSERTABLE IN THE EXTERNAL EAR



(57) Abstract: A cochlear implant system has a signal processor (50) that fits in the ear canal of a user. The signal processor (50) processes an acoustic signal present in the ear of the user to produce a representative radio signal. A power transmitter transmits an electrical power signal through the skin of the user. A cochlear implant receives the radio signal and the electrical power signal and produces for the auditory nerve of the user an electrical stimulation signal representative of the acoustic signal.

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For two-letter codes and other abbreviations, refer to the "Guidance Notes on Codes and Abbreviations" appearing at the beginning of each regular issue of the PCT Gazette.

COCHLEAR IMPLANT SYSTEM PARTIALLY INSERTABLE IN THE EXTERNAL EAR

Field of the Invention

5 The invention relates to a hearing prosthesis system using a cochlear implant.

Background Art

Deafness may be due to total sensorineural hearing loss. This is where the 10 cochlea does not respond to sound waves, and therefore does not generate electrical signals for transmission to the cochlear nerves. An auditory prosthesis may use a suitable stimulation electrode arrangement capable of stimulating the auditory nerves. One current prosthesis design includes an external transmitter and battery, and an internal receiver. The receiver interacts with electrodes that 15 are surgically placed in the cochlea to allow selective stimulation of the cochlear wall (Hochmair et al., U.S. Pat. No. 4,284,856 and 4,357,497, incorporated herein by reference). The electrodes are typically contained in a substantially flexible electrode carrier having sufficient stiffness to be guided into the cochlea in the desired coiled shape (Hochmair-Desoyer et al., Annals of the New York Academy 20 of Sciences 405:173-182 (1991), incorporated herein by reference).

Figure 1 shows a section view of an ear with a typical cochlear implant system. A normal ear transmits sounds through the outer ear 10 to the eardrum 12, which moves the bones of the middle ear 14, which in turn excites the cochlea 16. The cochlea 16 includes an upper channel, known as the scala vestibuli 18, 25 and a lower channel, known as the scala tympani 20, which are connected by the cochlear duct 22. In response to received sounds transmitted by the middle ear 14, the fluid filled scala vestibuli 18 and scala tympani 20 transmit waves, functioning as a transducer to generate electric pulses that are transmitted to the cochlear nerve 24, and ultimately to the brain.

To overcome total sensorineural hearing loss, a cochlear implant system produces direct electrical stimulation of the cochlea 16. A typical system may include an external microphone that provides an audio signal input to a signal processing stage (not shown) where various signal processing schemes can be 5 implemented. For example, signal processing approaches that are well-known in the field of cochlear implants include continuous interleaved sampling (CIS) digital signal processing, channel specific sampling sequences (CSSS) digital signal processing (as described in co-pending U.S. patent application 09/648,68, filed August 25, 2000, and incorporated herein by reference), spectral peak 10 (SPEAK) digital signal processing, and compressed analog (CA) signal processing. Typically, the processed signal is then converted into a digital data format, such as a sequence of data frames, for transmission into an implanted receiver 39.

Besides getting the processed audio information to the implanted receiver 39, existing cochlear implant systems also need to deliver electrical power from 15 outside the body through the skin to satisfy the power requirements of the implanted portion of the system. Figure 1 shows an arrangement based on inductive coupling through the skin to transfer both the required electrical power and the processed audio information. As shown in Fig. 1, a primary coil 38 (connected to the external signal processor) is externally placed adjacent to a 20 subcutaneous secondary coil 34 (connected to the receiver 39). This arrangement inductively couples a radio frequency (rf) electrical signal to the receiver 39.

The receiver 39 is able to extract both a power component from the rf signal it receives, and the audio information for the implanted portion of the system. Besides extracting the audio information, the receiver 39 also performs additional 25 signal processing such as error correction, pulse formation, etc., and produces a stimulation pattern (based on the extracted audio information) that is sent through connected wires 44 to an implanted electrode carrier 46. Typically, this electrode carrier 46 includes multiple electrodes on its surface that provide selective stimulation of the cochlea 16.

The transmission rf signal for primary coil 38 is typically provided by a prominent behind-the-ear (BTE) module. This BTE module may also contain other system components such as the microphone and the external signal processing arrangement. The BTE module may be quite visually obtrusive, and it

5 is known that some wearers of such devices are very sensitive that their appearance is abnormal.

Summary of the Invention

A representative embodiment of the present device includes a signal processing device for a cochlear implant. The device body fits into the ear canal of a user. The device body includes a microphone, a signal processor, and a transmitter. The microphone converts an acoustic signal present at the device body into a representative electrical signal. The signal processor performs signal processing of the representative electrical signal to form a cochlear implant signal.

10 The transmitter converts the cochlear implant signal into a radio signal for transmission to a cochlear implant.

15

Another embodiment includes a cochlear implant system that has a signal processor that fits in the ear canal of a user. The signal processor processes an acoustic signal present in the ear of the user to produce a representative radio signal. A separate power transmitter transmits an electrical power signal through the skin of the user. A cochlear implant receives the radio signal and the electrical power signal and produces for the auditory nerve of the user an electrical stimulation signal representative of the acoustic signal.

20

In further embodiments, the device body may include a mechanical stimulation module that delivers to the inner ear structure of the user a mechanical stimulation signal representative of a portion of the acoustic signal. In such a device the cochlear implant signal is representative of a first subrange of frequencies in the acoustic signal, and the mechanical stimulation signal is representative of a second subrange of frequencies in the acoustic signal.

25

The processing performed by the signal processor may include at least one of compression, beamforming, and filtering. The signal processing may be continuous interleaved sampling (CIS) digital signal processing, channel specific sampling sequences (CSSS) digital signal processing, spectral peak (SPEAK) 5 digital signal processing, or compressed analog (CA) signal processing.

An implanted battery module may power the cochlear implant, and the battery module may be rechargeable responsive to the transmitted electrical power signal.

The cochlear implant may use extracochlear electrodes to deliver the 10 electrical stimulation signal. Alternatively, cochleostomy window associated electrodes may deliver the electrical stimulation signal. Or, multi-channel array electrodes may be partially or fully inserted into the cochlea of the user to deliver the electrical stimulation signal.

Another embodiment includes a cochlear implant system having a power 15 transmitter that transmits an electrical power signal through the skin of the user, and a cochlear implant. The cochlear implant includes (i) a battery module that powers the cochlear implant, and that is rechargeable responsive to the transmitted electrical power signal, and (ii) a signal processor including a microphone. The signal processor processes an acoustic signal present in the ear 20 of the user, and produces for the auditory nerve of the user an electrical stimulation signal representative of the acoustic signal.

Brief Description of the Drawings

The present invention will be more readily understood by reference to the 25 following detailed description taken with the accompanying drawings, in which:

Figure 1 illustrates a section view of an ear connected to a cochlear implant system.

Figure 2 shows a top and a side view of an in-the-ear processor according to one specific embodiment of the present invention.

Detailed Description of Specific Embodiments

Various embodiments of the present invention are directed to a cochlear implant system that replaces the signal processing stage of the behind-the-ear (BTE) module of previous systems with an in-the-ear (ITE) module. This approach splits the power- and information-transfer functions to the implant into two independent transmission channels. Information transfer between the ITE processor and the implant uses a radio frequency (rf) connection. Power transfer uses the conventional inductively coupled coils. The transmitted power may be used to drive the implant, or implanted batteries may be recharged.

The ITE processor may be based on a conventional hearing aid, which is enhanced by an rf transmitter to communicate the audio information to the implant. Besides providing an audio signal to the implant for electrical stimulation of the auditory nerve, the ITE may also provide an acoustic mechanical stimulation module. This module can mechanically drive either the normal auditory chain of ear drum, middle ear, etc., or the round window from a cochleostomy. Such a combination of electric and mechanical auditory stimulation is described, for example, in application 09/258,997, filed February 26, 1999, which is commonly assigned and incorporated herein by reference.

Combined electric and mechanical stimulation can be particularly effective in cochlear implant patients who retain some residual hearing. Typically, the electrical stimulation provides audio information in a first range of frequencies, e.g., higher frequencies, and the mechanical stimulation provides audio information in a second range of frequencies, e.g., lower frequencies.

Figure 2 shows a top and a side view of an in-the-ear processor according to one specific embodiment of the present invention. The ITE processor 50 looks like a conventional hearing aid that is inserted into the ear canal in the outer ear, 10 in Fig. 1. A tapered inner end 52 slides into the ear canal of the outer ear 10 until it mechanically engages the eardrum 12. Figure 2 shows the tapered inner

end 52 as having a generic taper suitable for most users, but it is also known to make a custom molding of the ear canal of the outer ear 10 of the user, and to use this custom molding as the shape of the tapered inner end 52. In an embodiment having an acoustic mechanical stimulation module, the mechanical drive signal 5 may be provided via the tapered inner end 52. Alternatively, the tapered end 52 may be adapted to mechanically drive the round window from a cochleostomy.

The ITE processor 50 contains conventional digitally programmable hearing aid processing circuitry for processing tasks such as compression, beamforming, filtering, remote control, etc. The outer end 54 of the ITE processor 10 50 may be adapted to have various user accessible controls as shown to provide some user control over the processing, and more generally, operation of the system. Also within the case of the ITE processor 50 are the rf transmitter and the battery.

To cooperate with the ITE processor 50, the receiver, 39 in Fig. 1, contains 15 signal processing circuits to receive and extract the rf audio information signals from the transmitter. The extracted audio information is then processed by the receiver 39 into electrode stimulation signals, which are communicated via connecting wires 44 to the implanted electrode carrier 46 to provide electrical stimulation to the cochlea 16.

20 Various signal processing strategies are known in the art for stimulating the implanted electrodes in the electrode carrier 46. These include continuous interleaved sampling (CIS), channel specific sampling sequences (CSSS), spectral peak (SPEAK), and compressed analog (CA) processing. Other processing and stimulation strategies are known, and new strategies are likely to be developed in 25 the future; these are all within the scope of embodiments of the present invention.

Since both the ITE processor 50 and the receiver 39 contain signal processing components, specific embodiments vary as to how much processing is performed by each. For example, in a one system using CIS processing, the ITE processor 50 produces a minimally processed analog audio signal for the

subcutaneous receiver 39. In other embodiments, the audio signal from the ITE processor 50, while still analog, may have more sophisticated analog signal processing performed on it; for example, automatic gain control (AGC) and beamforming such as is done in a conventional hearing aid. Typical methods for 5 transmitting an analog audio signal include well-known techniques such as amplitude modulation (AM) or frequency modulation (FM). In any case, the receiver 39 processes the received analog audio information using the CIS digital signal processing technique, and produces a stimulation signal for the electrodes of the implanted electrode carrier 46.

10 But, in an alternative embodiment, the ITE processor 50 also may perform analog to digital conversion of the audio signal, followed by digital signal processing. For instance, the ITE processor 50 may transmit to the receiver 39 a sequence of digital data frames containing the information necessary to reconstruct the analog audio signal. Typical methods for transmitting a digital 15 audio signal include such well-known techniques as amplitude shift keying (ASK), frequency shift keying (FSK), and phase shift keying (PSK). The receiver 39 may then perform CIS processing of the received digital signal and construct an electrode stimulation pattern based on the information in the received digital data signal. Alternatively, the ITE processor 50 may further process the digital 20 audio signal to produce the CIS pulse information, which is then converted into a sequence of digital frames and transmitted to the receiver 39. The receiver 39 then uses the information in the received digital frame sequence to construct the CIS pulse pattern for the implanted electrodes.

Similar shifting of signal processing functionality between the ITE 25 processor 50 and the receiver 39 may be used in other specific embodiments based on other signal processing strategies. Moreover, the information channel to the receiver 39 can be used by other devices than the ITE processor 50. For example, using the rf frequency of the receiver 39 and the proper audio information format,

a telephone, television, radio, or other external audio device could transmit an audio signal to the receiver 39.

In representative embodiments, the receiver 39 may contain rechargeable batteries. With such an arrangement, a behind-the-ear (BTE) module may be used

5 at night while the user is sleeping to inductively couple electrical power from primary coil 38 through the skin to secondary coil 34 to recharge the batteries in the receiver 39 while the user is asleep. Then, in the morning, the user can remove the BTE module and rely on the recharged batteries in the receiver 39 to provide electrical power throughout the day to the implanted portion of the

10 system. Alternatively, a rechargeable battery module may be implanted separately from the receiver 39. Using an implanted battery, there is no prominently visible external module, only the unobtrusive ITE processor, which appears to be a conventional hearing aid.

In another alternative embodiment, implanted rechargeable batteries are

15 not used. Rather, the previously known inductive coupling arrangement is used to provide electrical power to the implanted portion of the system. And, if the all the signal processing is performed by the implanted portion of the system, the ITE processor may omitted altogether by also implanting a microphone in communication with the implanted receiver. Thus, power transmission and

20 information transmission and processing are still kept as separate functions transmitted over separate channels. This arrangement allows for a low profile BTE module that may be covered by the user's hair, and which contains just an external battery and the power transmission components. These parts can be made to be very robust and inexpensive, and servicing is greatly simplified.

25 In another alternative embodiment, an external signal processing module may be added to the external part of the power transmission system. An rf receiver within this module receives and processes the audio information sent by the transmitter in the ITE processor. The processed audio is then modulated into

the power transmission signal, which has enough rf-bandwidth to transmit broadband stimulation data.

The foregoing discussion has described various advantages of representative embodiments of the present invention over existing cochlear implant systems that use an external BTE or body-worn processor. It should be noted that the various embodiments also offer significant advantages over fully implanted cochlear implant systems that have no external components. For example, the surgery to place the implanted portions of the system is less complicated than in a fully implanted system that surgically implants a microphone in the ear canal. Also, the location of the microphone in the ITE processor can be acoustically optimized compared to a system that integrates the microphone into the implant package. And, newly emerging signal processing strategies can be readily implemented in the ITE processor as they become available. This is not possible if the processing circuits are fully implanted.

Although various exemplary embodiments of the invention have been disclosed, it should be apparent to those skilled in the art that various changes and modifications can be made which will achieve some of the advantages of the invention without departing from the true scope of the invention.

What is claimed is:

- 1 1. A signal processing device for a cochlear implant, the device comprising:
 - 2 a device body that fits into the ear canal of a user, the device body
 - 3 containing:
 - 4 (i) a microphone that converts an acoustic signal present at the
 - 5 device body into a representative electrical signal;
 - 6 (ii) a signal processor that performs signal processing of the
 - 7 representative electrical signal to form a cochlear implant signal;
 - 8 and
 - 9 (iii) a transmitter that converts the cochlear implant signal into a
 - 10 radio signal for transmission to a cochlear implant.
- 1 2. A device according to claim 1, wherein the device body further includes:
 - 2 a mechanical stimulation module that delivers to the inner ear structure
 - 3 of the user a mechanical stimulation signal representative of a
 - 4 portion of the acoustic signal,
 - 5 wherein the cochlear implant signal is representative of a first subrange
 - 6 of frequencies in the acoustic signal, and the mechanical
 - 7 stimulation signal is representative of a second subrange of
 - 8 frequencies in the acoustic signal.
- 1 3. A device according to claim 1, wherein the processing performed by the
- 2 signal processor includes at least one of compression, beamforming, and
- 3 filtering.
- 1 4. A device according to claim 1, wherein the signal processing includes
- 2 continuous interleaved sampling (CIS) digital signal processing.

- 1 5. A device according to claim 1, wherein the signal processing includes
2 channel specific sampling sequences (CSSS).
- 1 6. A device according to claim 1, wherein the signal processing includes
2 spectral peak (SPEAK) digital signal processing.
- 1 7. A device according to claim 1, wherein the signal processing includes
2 compressed analog (CA) signal processing.
- 1 8. A cochlear implant system comprising:
 - 2 a signal processor that fits in the ear canal of a user and processes an
3 acoustic signal present in the ear of the user to produce a
4 representative radio signal;
 - 5 a power transmitter that transmits an electrical power signal through
6 the skin of the user; and
 - 7 a cochlear implant that receives the radio signal and the electrical
8 power signal and produces for the auditory nerve of the user an
9 electrical stimulation signal representative of the acoustic signal.
- 1 9. A system according to claim 8, wherein the signal processor further includes:
 - 2 a mechanical stimulation module that delivers to the inner ear structure
3 of the user a mechanical stimulation signal representative of a
4 portion of the acoustic signal, wherein the cochlear implant signal
5 is representative of a first subrange of frequencies in the acoustic
6 signal, and the mechanical stimulation signal is representative of
7 a second subrange of frequencies in the acoustic signal
- 1 10. A system according to claim 8, further comprising:
 - 2 an implanted battery module that powers the cochlear implant, and
3 that is rechargeable responsive to the transmitted electrical power

4 signal.

- 1 11. A system according to claim 8, wherein the processing performed by the
- 2 signal processor includes at least one of compression, beamforming, and
- 3 filtering.
- 1 12. A system according to claim 8, wherein the processing performed by the
- 2 signal processor includes continuous interleaved sampling (CIS) digital
- 3 signal processing.
- 1 13. A system according to claim 8, wherein the processing performed by the
- 2 signal processor includes channel specific sampling sequences (CSSS).
- 1 14. A system according to claim 8, wherein the processing performed by the
- 2 signal processor includes spectral peak (SPEAK) digital signal processing.
- 1 15. A system according to claim 8, wherein the processing performed by the
- 2 signal processor includes compressed analog (CA) signal processing.
- 1 16. A system according to claim 8, wherein the cochlear implant uses
- 2 extracochlear electrodes to deliver the electrical stimulation signal.
- 1 17. A system according to claim 8, wherein the cochlear implant uses
- 2 cochleostomy window associated electrodes to deliver the electrical
- 3 stimulation signal.
- 1 18. A system according to claim 8, wherein the cochlear implant uses multi-
- 2 channel array electrodes partially inserted into the cochlea of the user to
- 3 deliver the electrical stimulation signal.
- 1 19. A system according to claim 8, wherein the cochlear implant uses multi-

2 channel array electrodes fully inserted into the cochlea of the user to deliver
3 the electrical stimulation signal.

1 **20. A cochlear implant system comprising:**

2 a power transmitter that continuously transmits an electrical power
3 signal through the skin of the user; and

4 a cochlear implant having

5 (i) a power processing module that continuously provides power to
6 the cochlear implant responsive to and representative of the
7 transmitted electrical power signal, and
8 (ii) a signal processor including a microphone, the signal processor
9 processing an acoustic signal present in the ear of the user and
10 producing for the auditory nerve of the user an electrical
11 stimulation signal representative of the acoustic signal.

1 **21. A system according to claim 20, wherein the processing performed by the**
2 **signal processor includes at least one of compression, beamforming, and**
3 **filtering.**

1 **22. A system according to claim 20, wherein the processing performed by the**
2 **signal processor includes continuous interleaved sampling (CIS) digital**
3 **signal processing.**

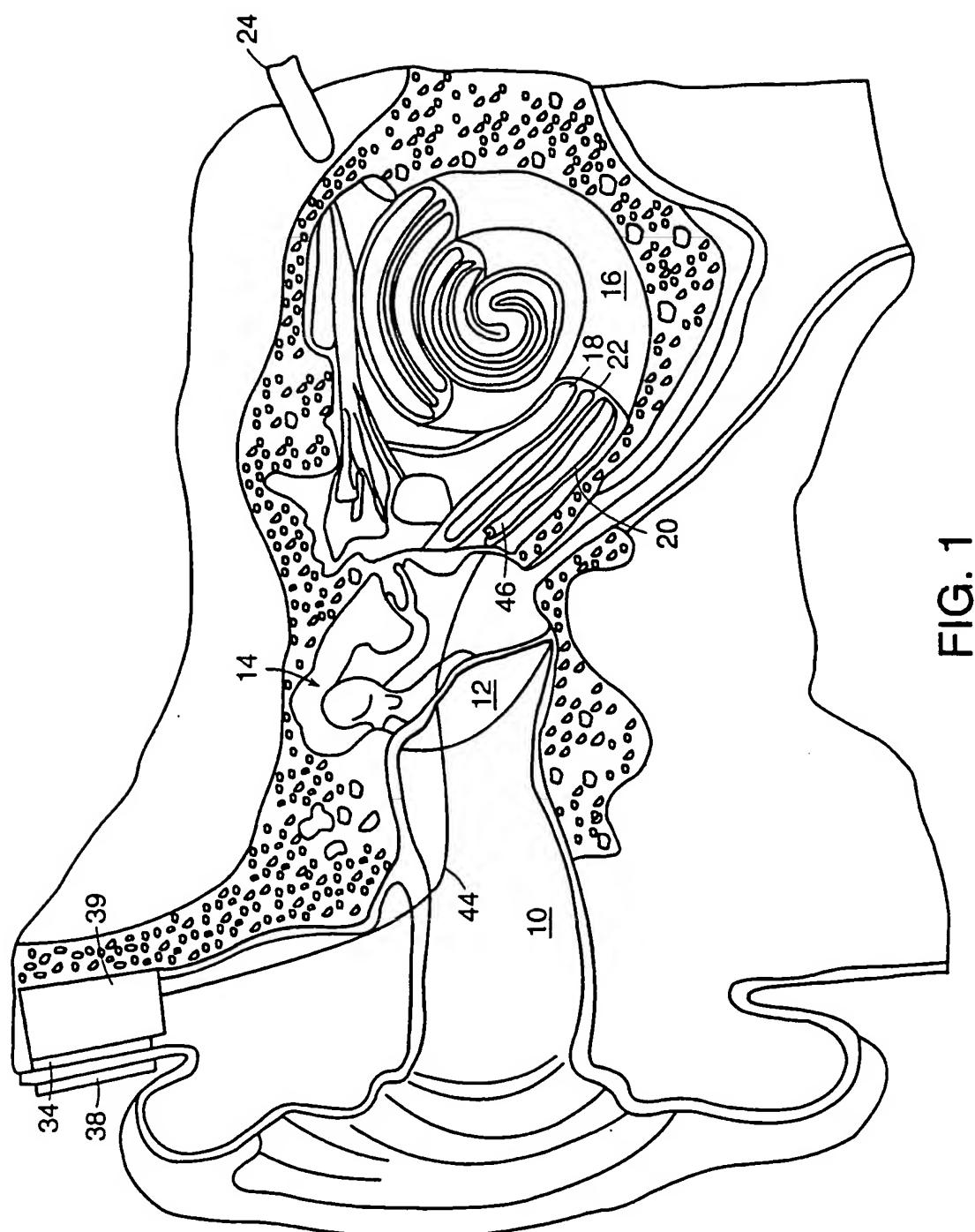
1 **23. A system according to claim 20, wherein the processing performed by the**
2 **signal processor includes channel specific sampling sequences (CSSS).**

1 **24. A system according to claim 20, wherein the processing performed by the**
2 **signal processor includes spectral peak (SPEAK) digital signal processing.**

1 **25. A system according to claim 20, wherein the processing performed by the**
2 **signal processor includes compressed analog (CA) signal processing.**

- 1 26. A system according to claim 20, wherein the cochlear implant uses
- 2 extracochlear electrodes to deliver the electrical stimulation signal.
- 1 27. A system according to claim 20, wherein the cochlear implant uses
- 2 cochleostomy window associated electrodes to deliver the electrical
- 3 stimulation signal.
- 1 28. A system according to claim 20, wherein the cochlear implant uses multi-
- 2 channel array electrodes partially inserted into the cochlea of the user to
- 3 deliver the electrical stimulation signal.
- 1 29. A system according to claim 20, wherein the cochlear implant uses multi-
- 2 channel array electrodes fully inserted into the cochlea of the user to deliver
- 3 the electrical stimulation signal.

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FIG.

2/2

FIG. 2B

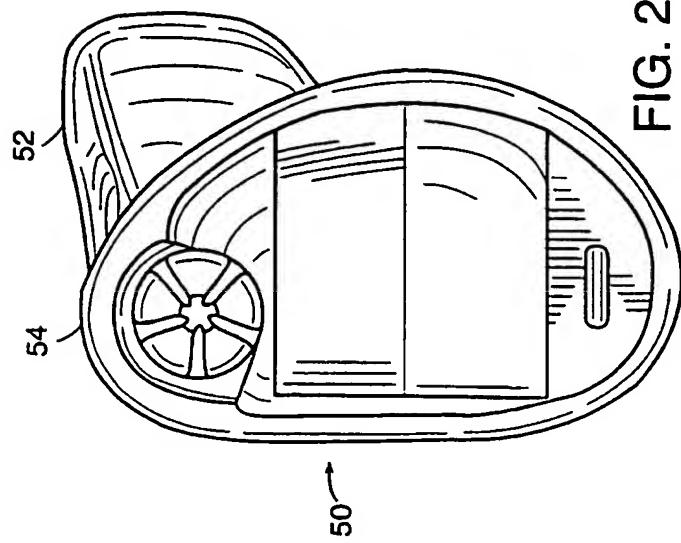
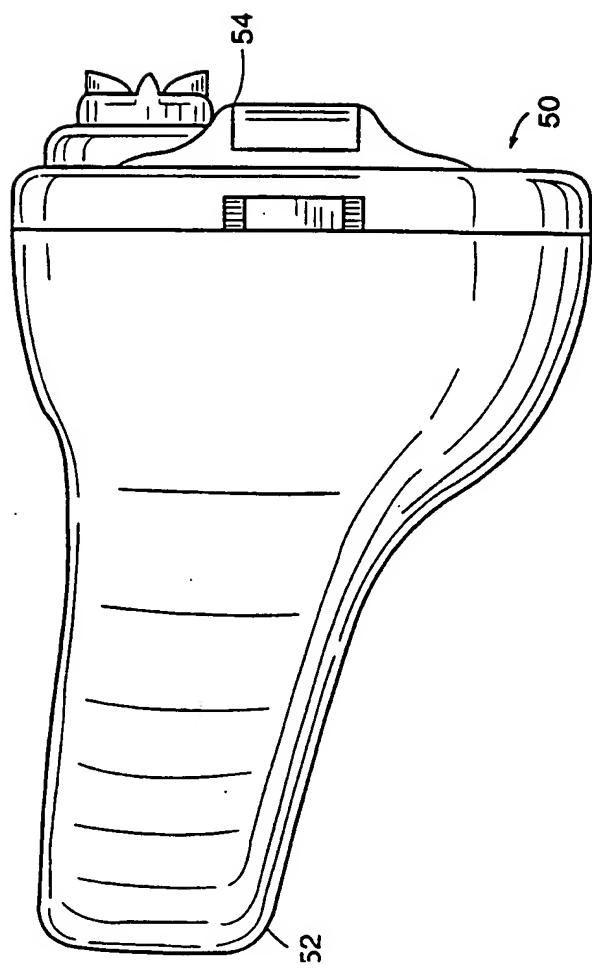


FIG. 2A



INTERNATIONAL SEARCH REPORT

International Application No
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A. CLASSIFICATION OF SUBJECT MATTER		
IPC 7 A61F11/04 A61N1/36 H04R25/00 H04R25/02		
According to International Patent Classification (IPC) or to both national classification and IPC		
B. FIELDS SEARCHED		
Minimum documentation searched (classification system followed by classification symbols)		
IPC 7 A61F A61N H04R		
Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched		
Electronic data base consulted during the international search (name of data base and, where practical, search terms used)		
WPI Data, PAJ, EPO-Internal		
C. DOCUMENTS CONSIDERED TO BE RELEVANT		
Category	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
A	US 4 817 607 A (TATGE GARY) 4 April 1989 (1989-04-04) column 4, line 11 -column 6, line 47 claim 1; figures 1-4 ---	1,2
A	US 5 558 618 A (MANIGLIA ANTHONY J) 24 September 1996 (1996-09-24) claims 11-19; figures 19,21 ---	1,2
A	US 5 800 336 A (DIETZ TIM ET AL) 1 September 1998 (1998-09-01) column 21, line 16 - line 28 claims; figure 20C ---	1,2 -/-
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International Application No
PCT/IB 01/00455

C.(Continuation) DOCUMENTS CONSIDERED TO BE RELEVANT		
Category	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
A	GEORGE C R: "COCHLEAR IMPLANTS: TECHNOLOGY FOR THE PROFOUNDLY DEAF" MEASUREMENT AND CONTROL, vol. 26, no. 9, 1 November 1993 (1993-11-01), pages 267-270, XP000416746 LONDON, GB ISSN: 0020-2940 the whole document ---	1-29
A	US 4 739 512 A (HARTL CHRISTOF ET AL) 19 April 1988 (1988-04-19) claims; figures 1-7 ---	1,8,20
A	US 4 284 856 A (HOCHMAIR INGEBORG J ET AL) 18 August 1981 (1981-08-18) cited in the application the whole document ---	1
A	US 4 357 497 A (HOCHMAIR INGEBORG J ET AL) 2 November 1982 (1982-11-02) cited in the application the whole document ---	1
A	HOCHMAIR-DESOYER IJ ET AL: "Design and fabrication of multiwire scala tympani electrodes" ANNALS OF THE NEW YORK ACADEMY OF SCIENCES, vol. 405, 1983, pages 173-182, XP001009521 New York US cited in the application the whole document -----	

INTERNATIONAL SEARCH REPORT

Information on patent family members

International Application No

PCT/IB 01/00455

Patent document cited in search report	Publication date	Patent family member(s)			Publication date
US 4817607	A 04-04-1989	US 4800884 A			31-01-1989
		AU 603896 B			29-11-1990
		AU 1617988 A			17-11-1988
		CA 1328228 A			05-04-1994
		DE 3888570 D			28-04-1994
		DE 3888570 T			29-09-1994
		EP 0291325 A			17-11-1988
		ES 2053731 T			01-08-1994
		JP 63309099 A			16-12-1988
		AU 606588 B			14-02-1991
		AU 6982187 A			10-09-1987
		CA 1277761 A			11-12-1990
		DE 3788529 D			03-02-1994
		DE 3788529 T			16-06-1994
		EP 0242038 A			21-10-1987
		JP 63159000 A			01-07-1988
		US 4840178 A			20-06-1989
US 5558618	A 24-09-1996	US 5906635 A			25-05-1999
US 5800336	A 01-09-1998	US 5913815 A			22-06-1999
		US 5624376 A			29-04-1997
		US 5554096 A			10-09-1996
		US 5456654 A			10-10-1995
		US 5795287 A			18-08-1998
		US 5897486 A			27-04-1999
		EP 0801878 A			22-10-1997
		JP 11506572 T			08-06-1999
		AU 4695996 A			24-07-1996
		WO 9621335 A			11-07-1996
		US 5857958 A			12-01-1999
		AU 683671 B			20-11-1997
		AU 7179594 A			24-01-1995
		CA 2165557 A			12-01-1995
		EP 0732035 A			18-09-1996
		JP 8512182 T			17-12-1996
		WO 9501710 A			12-01-1995
		US 6190305 B			20-02-2001
US 4739512	A 19-04-1988	DE 8518681 U			12-06-1986
		AT 56848 T			15-10-1990
		CA 1258434 A			15-08-1989
		DE 3674260 D			25-10-1990
		DK 298186 A			28-12-1986
		EP 0206213 A			30-12-1986
		JP 1825335 C			28-02-1994
		JP 5030360 B			07-05-1993
		JP 62002800 A			08-01-1987
US 4284856	A 18-08-1981	AT 371660 B			25-07-1983
		AT 446180 A			15-11-1982
		CH 657984 A			15-10-1986
		DE 3034394 A			09-04-1981
		FR 2465474 A			27-03-1981
		GB 2061733 A, B			20-05-1981
		US 4357497 A			02-11-1982
US 4357497	A 02-11-1982	US 4284856 A			18-08-1981

INTERNATIONAL SEARCH REPORT

Information on patent family members

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Patent document cited in search report	Publication date	Patent family member(s)		Publication date
US 4357497	A	AT	371660 B	25-07-1983
		AT	446180 A	15-11-1982
		CH	657984 A	15-10-1986
		DE	3034394 A	09-04-1981
		FR	2465474 A	27-03-1981
		GB	2061733 A,B	20-05-1981